Biosensori bazîndu-se pe Magneto-resistența

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Bio-Assay Technology

Magnetic Bio-Assay Technology

Tunnelling Magneto-resistance sensor

Magnetotactic Bacteria

Targeting by MRI

Conclusions

Microarrays

Molecular probes immobilised on small spots on a substrate. Position is used to distinguish different probes.

Spatially resolved fluorescence is used to detect hybridisation -> bulky and expensive optics needed.

The GeneChip (Affymetrix) is used to search for millions of targets at once. But, arrays are expensive to customise and can not be modified post production.

2D kinetics limits sensitivity and increases run-time for multiplexed assays.

medical applications: a review", in Med. and Bio. Eng. and Comp. (Springer, 2010) Doi:10.1007/s11517-010-

J. Llandro, J.J. Palfreyman, **A. lonescu** and C.H.W. Barnes, Invited: "*Magnetic biosensor technologies for* 0643-3.









 Molecular probes are attached to microcarriers which mix in a solution.
3D-Kinetics increases sensitivity and decreases run-time.

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➢ For multiplexing, each particle is labelled in to uniquely identify the probe.

Most encoding systems are graphical or fluorescent bead based, e.g. xMAP (Luminex) and QuantumDot (Invitrogen).

SAT's are limited by the number of codes generated and expensive optics to read them.



"Quantum-dot-tagged microbeads for multiplexed optical coding of biomolecules", M. Han, X. Gao, J. Z. Su and S. Nie, Nature Biotechnology **19**, 631 (2001).

CAMBRIDGE Multiplexing Technologies

Encoded Particles – Pregibon *et al., Science* **315**, 1393 (2007).

Nanowires – Nicewarner-Peña *et al., Science* **294**, 137 (2001).



Diffraction Gratings – Broder *et al., Anal. Chem.* **80** (6), 1902 (2008).





Optical labelling

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- Reading the labels requires frequency or spatial resolution and so bulky and expensive optics are often necessary.
- Microcarriers are made with the labels pre-written.
- Multiplexing can be expensive due to the need for parallel fabrication.
- Number of labels available for fluorescence based techniques is limited due to the overlap of emission spectra.
- Autofluorescence in the sample can increase signal-to-noise ratio.

Magnetic labelling

- Codes may be read using integrated GMR/TMR devices, similar to those used in hard drives.
- The code can be written and rewritten using a magnetic field.
- All the microcarriers can be manufactured identically using MEMS techniques reducing costs.
- Scalable: number of available labels increases exponentially with each element in a digital architecture, *i.e.* each additional bit doubles the coding capacity.
- Biological samples have a very low magnetic background.



Magnetic Barcodes

How can magnetic tagging offer multiplexing potential?







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All unique codes can be written using a global field that varies in amplitude. Tags with elements that switch at different field strengths can be written with a 'global' field.

> Enables to write a code on a large number of tags at any one time.

➤ However, the coercivity of magnetic elements must change for varying their switching fields.

Shape anisotropy (different aspect ratio) can be used to tune the coercivity.





1st Generation Tags



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The tags can be released from the substrate and biochemically functionalised...



...and controllably flown (and sorted) within microfluidic channels over buried sensors.

SU-8 Surface Chemistry

Simple epoxide ring opening under nucleophilic attack:

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2nd Generation Tags

Better fluorescent marker (TAMRA vs FITC)

Simpler fabrication procedure:

- Release layer is optional
- Only 1 alignment step (previously 2)

New chemistry (harder but more interesting):

- Novel SU8 etchant
- Chemical release from silicon wafer
- Spacer molecules



Microfluidic control: optical trapping via "mickey mouse" ears

Dimensions: 100µm x 30µm x 3µm









Micro-magnetic simulations suggest that a 200 μ m long planar tag can currently accommodate 13 bits \Rightarrow 8000 codes (great for SNPs/gene expression)

Vacuum chambers and multiple photolithography steps add to the fabrication costs cheaper methods would allow for mass production of billions of tags

3D Electrodeposited multilayer pillars offers an answer to all three areas:

- More Coding Capacity
- More Compact
- More Cost Effective



Multi-coercivity



Exchange-bias: magnetic elements are coupled to anti-ferromagnetic layers, thus changing the switching field.

4-bit sputtered film with layers:

 $[Co(3)/PdMn(x)/Ta(5)]_4$ where x = 13, 11, 9and 7 nm from bottom to top of the loop.

♦ <u>Height variation</u>: thicknesses from 5nm to several μ m can be grown by controlling the cut-off charge (electrodeposited).

SQUID magnetometry of 2-bit multicoercivity tags with structure:

Cu(50)/Co(50)/Cu(50)/Co(25)/Cu(25)



M. Barbagallo, F. van Belle, **A. Ionescu** and J.A.C. Bland, in *"Biomagnetism and Magnetic Biosystems based on Molecular recognition Processes"*, ed. **A. Ionescu** and J.A.C. Bland, *AIP Conf. Proc.* **1025**, 52 (2008).





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➤ Spacer molecules or DNA modified with a nucleophilic group can bind covalently to the magnetic tag.

➤ The release layer can be dissolved to allow suspension based hybridisation and detection/sorting/reading steps. A (di-)thiol based Self-Assembled
Monolayer with a functional head group can be grown on the gold cap layer, enabling further chemistry...



DNA Hybridisation

> Array of 15 μ m diameter pillars hybridised to fluorescently-labelled DNA ...



...proof that all 7 steps are working:

- ✓ Release layer(s) evaporated
- ✓ Photolithographically patterned
- ✓ Multilayer pillars electrodeposited
- ✓ Gold cap layer electrodeposited
- ✓ SAM grown
- \checkmark amino-DNA probe added
- ✓ hybridised to complementary fluorescent DNA.



However, this is just one DNA probe – how can we efficiently generate a large library?

J.J. Palfreyman, F. van Belle, J.A.C. Bland, M. Bradley et al. IEEE Trans. Mag. 43, 2439 (2007).

Split 'n' Mix Synthesis



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Giant/Tunnelling Magneto-resistance





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T.J. Hayward, J. Llandro, J.A.C. Bland, C.H.W. Barnes *et al.,* in *"Biomagnetism and Magnetic Biosystems based on Molecular recognition Processes",* ed. **A. Ionescu** and J.A.C. Bland, *AIP Conference Proceedings* **1025**, 111 (2008).



Integrated TMR Sensor



TMR sensors (*Micromagnetics Inc.*) with an active area of 2x5µm.

A dummy chip is used to mould a PDMS base with a cavity in which we can embed our TMR sensor chip. ➢ A PDMS channel is constructed using a lithographically defined SU-8 mould.

After the sensor is wire bonded the channel is aligned accurately over the sensor using a customised mask aligner.

TMR Detection: Measurements



The response of 5-bit tags in the (1,1,1,1,1) orientation [hardest to distinguish] were recorded passing over a TMR sensor buried under a 50µm microfluidic channel.











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N.J. Darton *et al.*, in *"Biomagnetism and Magnetic Biosystems based on Molecular recognition Processes"*, ed. **A. Ionescu** and J.A.C. Bland, *AIP Conference Proceedings* **1025**, 111 (2008).

100 nm HV-80.0kV Direct Mao: 14000

CAMBRIDGE CAMBRIDGE Culture of Magnetospirillum sp.



Magnetotactic bacteria found in the Cam!

- 1: Obligate aerobe (oxygen-needing)
- 2: Obligate anaerobe (avoid oxygen)
- 3: Facultative bacteria (aerobic respiration preferred)
- 4: Microaerophiles (require oxygen at low concentration)
- 5: Aerotolerant bacteria (not affected by oxygen)







CAMBRIDGE TEM of Magnetospirillum sp.





Mean nanoparticle size from 237 measurements = 51 13 nm

A. Ionescu, N.J. Darton, J. Llandro and K. Vyas , Invited: *Philosophical Transactions of the Royal Society A* **368**, 4371 (2010).



SQUID Magnetometry



Langevin Equation:
$$\sigma = Nm\mu_B \left(\cot \left(\frac{m\mu_B H}{k_B T} \right) - \frac{k_B T}{m\mu_B H} \right) + \chi_p H$$

Static TMR Measurements



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CAMBRIDGE Manipulation & Tracking of SP Nanoparticles using MRI



Chemical Characterisation: High Resolution Transmission Electron Microscopy



N.J. Darton , R.D. Hallmark, A. lonescu et al., Nanotechnology 19, 395102 (2008).







Fridge magnet for targeting

Targeted retroviral gene delivery

Targeted mammalian cell patterning

N.J. Darton *et al.*, in *"Biomagnetism and Magnetic Biosystems based on Molecular recognition Processes"*, ed. **A. Ionescu** and J.A.C. Bland, *AIP Conference Proceedings* **1025**, 111 (2008).

Targeting by MRI

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Targeting by MRI

Magnetic field gradient G _z (T m ⁻¹)	Magnetic force <i>F_{mag}</i> (N)	Observed velocity (mm s ⁻¹)	Expected velocity v _E (mm s ⁻¹)	Predicted agglomerate size (µm)
0.61	$3.7 imes 10^{-20}$	0.3	0.17 × 10 ⁻⁶	17
1.21	$7.4 imes 10^{-20}$	2.8 leading edge	0.56 × 10 ⁻⁶	29
1.21	$7.4 imes 10^{-20}$	0.5 trailing edge	0.56 × 10 ⁻⁶	12
2.42	1.5 × 10 ⁻¹⁹	7.0	1.35 × 10 ⁻⁶	29



 $G_z = 0.61 \text{ T m}^{-1}$



Vertical axis

10 mm



 $G_z = 0 T m^{-1}$

time →



 $G_z = 2.42 \text{ T m}^{-1}$

Nanoparticles





Conclusions



Detection of endogenous magnetic nanoparticles (static/dynamic mode) by TMR. Detection of smallest magnetic entity so far reported.

Magnetic targeting with Magnetic Resonance Imaging.





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TFM Current:

Dr. Crispin H.W. Barnes Dr. Justin J. Palfreyman Dr. Justin Llandro Dr. Thanos Mitrelias Dr. Theodossis Trypiniotis Mr. Bingyan Hong Mr. Joshaniel F.K. Cooper Mr. Kunal N. Vyas

TFM Former:

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Chemical Engineering and Biotechnology, Cambridge University

Prof. Nigel Slater Dr. Nicholas J. Darton King's College, London

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Prof. Mark Bradley Dr. Maria Lopalco

Current Technologies

<u>Microarrays</u>

- Sensitivity limited by 2D geometry.
- Expensive to produce.

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- Can not be tailored to the application after production.
- Inflexible requiring bulky and expensive optics to operate.
- Can be highly multiplexed.



- Sensitivity is higher due to 3D microcarrier kinetics.
- Cost depends almost entirely on microcarrier design.
- Can be tailored somewhat after production.
- Equipment required depends on labelling architecture.
- Multiplexing is limited by number of labels generated.



Baseline Shift (SEM)



CAMBRIDGE Dynamic TMR Measurements





